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Applied  
Biomechanics

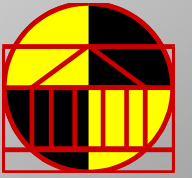
# *Injury Criteria and Numerical Modeling for High Speed Craft*

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*University of Virginia  
Center for Applied Biomechanics*

*February 2005*



# Overview

# Mk V SOC





# Scope

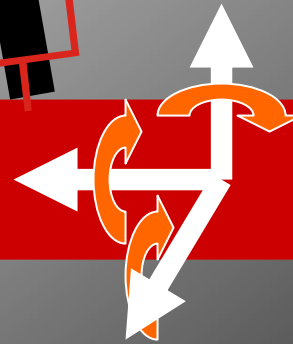
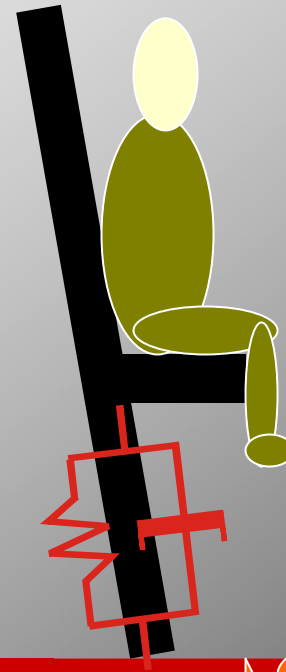
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- Prevention of Human Injury Should Be Included In the *Initial* Design Process
- Example: Automobile Impact Protection
  - Incorporated into initial design (Numerical Models)
  - Tested Using
    - Objective criteria (Head, Thorax, Femur Injury)
    - Established test protocol (Sled, Automobile Impact Tests)
  - Outcome checked using epidemiology (FARS, NASS)
  - The human is always part of the system
- Problem with High Speed Craft:  
*No Fully Suitable Injury Criterion*



# Human Dynamics Modeling

Seat/Body  
Dynamics



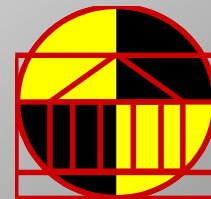
Hull/Deck Dynamics



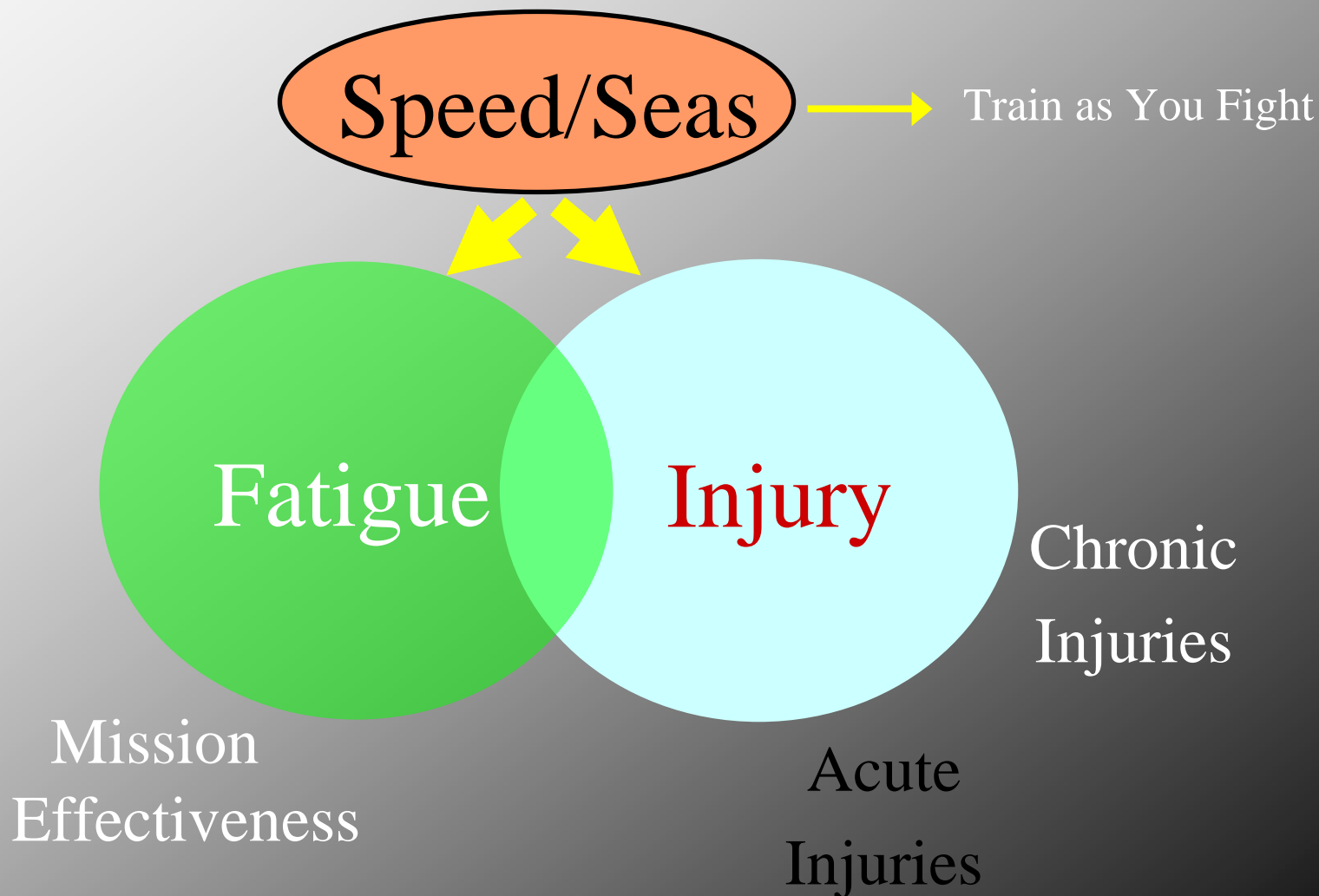
# Framework

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- Need => Validated Tools and Objective Measures of Goodness
- Robust Injury Model
  - Suitable for situation
- Numerical Models
  - Developing specifications, Initial craft design
  - Countermeasure development, Evaluation of procedures
- Experimental Validation
  - Evaluation of craft, numerical models
- Epidemiological Tracking
  - Injury investigations
  - Evaluation of injury models



# Injury Issues





# Other Considerations

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- Acute Injuries
  - Loss of personnel during rehabilitation
  - Potential immediate decrease in mission effectiveness
- Chronic Injuries
  - Pain, morale, loss of personnel during rehab
  - Long term consequences, costs
- Human Factors – Fatigue, Comfort, Workflow
  - Potentially long missions
  - Need for operators to remain mobile
- Additional Equipment
  - Night Vision/Helmet – Head mounted mass problem



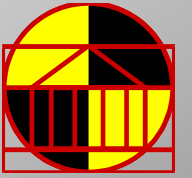
# Self Reported Injury Survey

- Example Epidemiological Study – Ensign *et al* (2000) NHRC
- Prevalence of Injury
  - 65% of SBU Operators Report At Least One Injury
  - Distribution of Injuries
    - Lower back, neck and upper back
    - Knee, Shoulder, Ankle
- Most Serious Injuries
  - Trauma
  - Fracture
  - **Intervertebral disc problems – particularly prominent**
- Impact of Injuries
  - 33% reported some limitations on mission performance
  - 44% reported limited duty days associated with injury

# Injuries in High Speed Boat Operators: Anecdotal Findings (*Bass et al - 2000*)



- No Reported Coccyx Injuries => No Lower Spine Blunt Impact Injuries
- Acute injuries
  - Often associated with momentary inattention to wave state
  - Irregular wave approach
- Chronic injuries not specifically associated with impact event
  - Often identified with an acute injury
- One Operator – Lower Spine Disc Herniation
  - 3200 mg ibuprofen daily – **self medicated!**



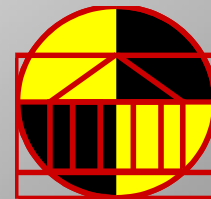
# Biomechanics



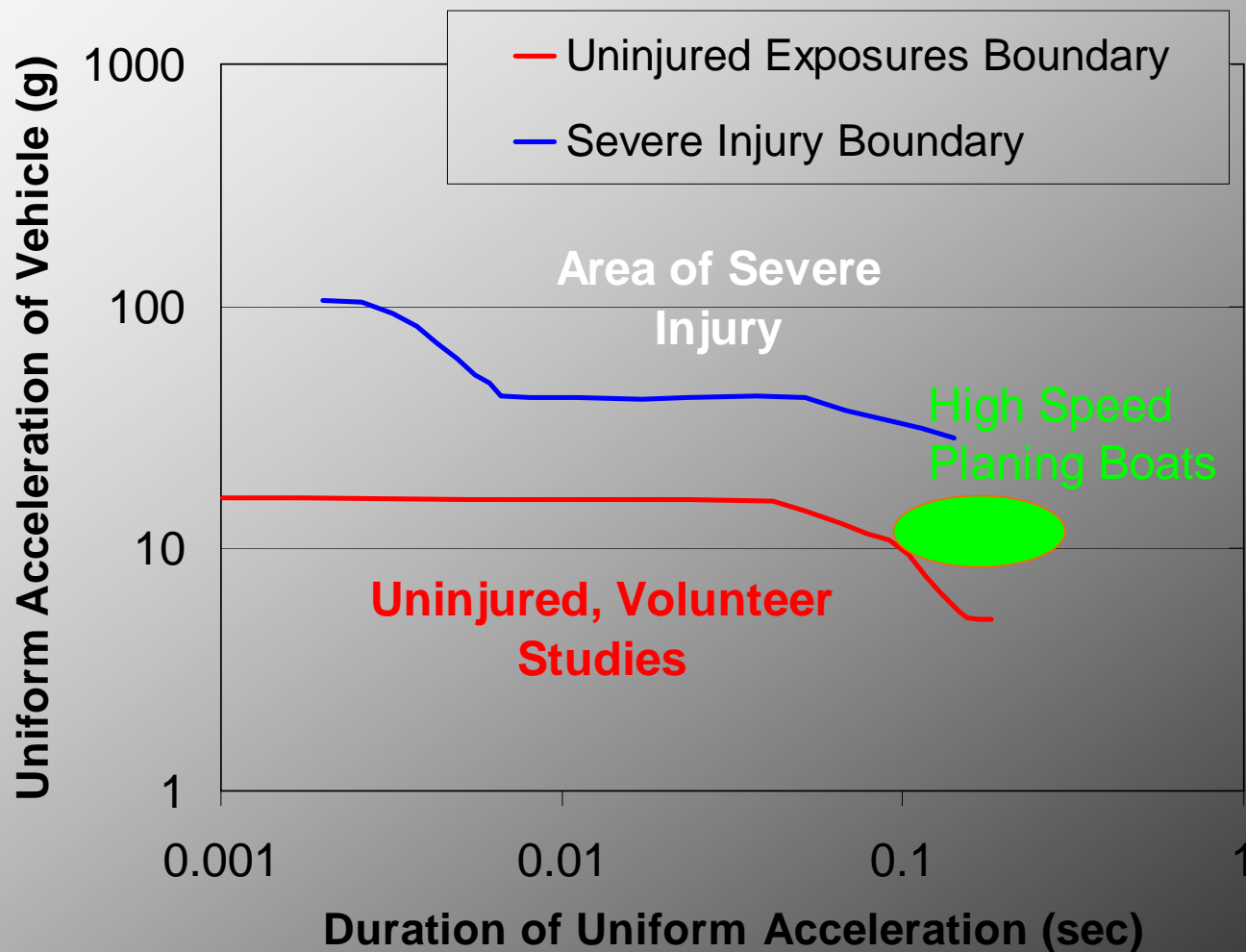
# Current Injury Criteria

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- Focus on ‘Biomechanical’ Criteria
  - Not ISO-2631 pt. 1, VDV etc
- Many – Often Acceleration Based
  - Surrogate for applied force
- None Are Completely Applicable to this Problem
  - Complex postures
  - Long term repeated/complex loading
- Often Outside the Range of Applicability



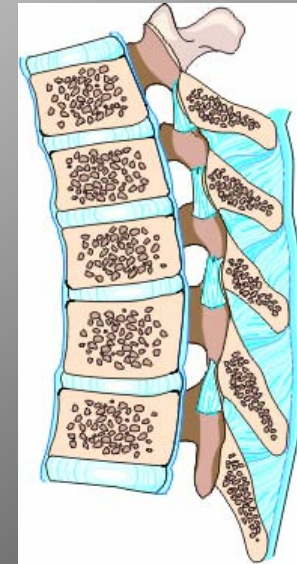
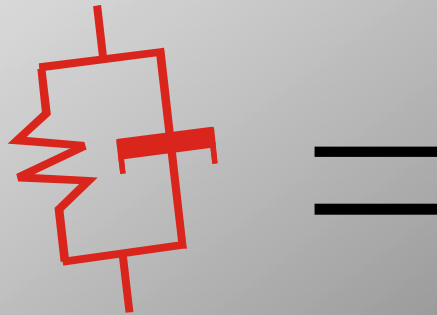
# Ejection Seats – Single Impact





# Displacement Response Index (DRI)

- Simple Lumped Mass Model, Ejection Injuries [Payne-1975]
- Compressive Loading => Compressive Fracture



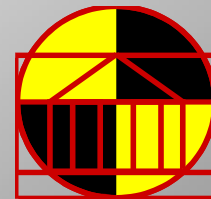
- WEDIM (Peterson-1996)
- Limited Usefulness
  - Does not account for repetitive loading  
(Extension not validated for  $n > 4$  impacts)
  - Based on compressive spinal fracture
  - Columnar spinal loading
  - Does not account for complex postures



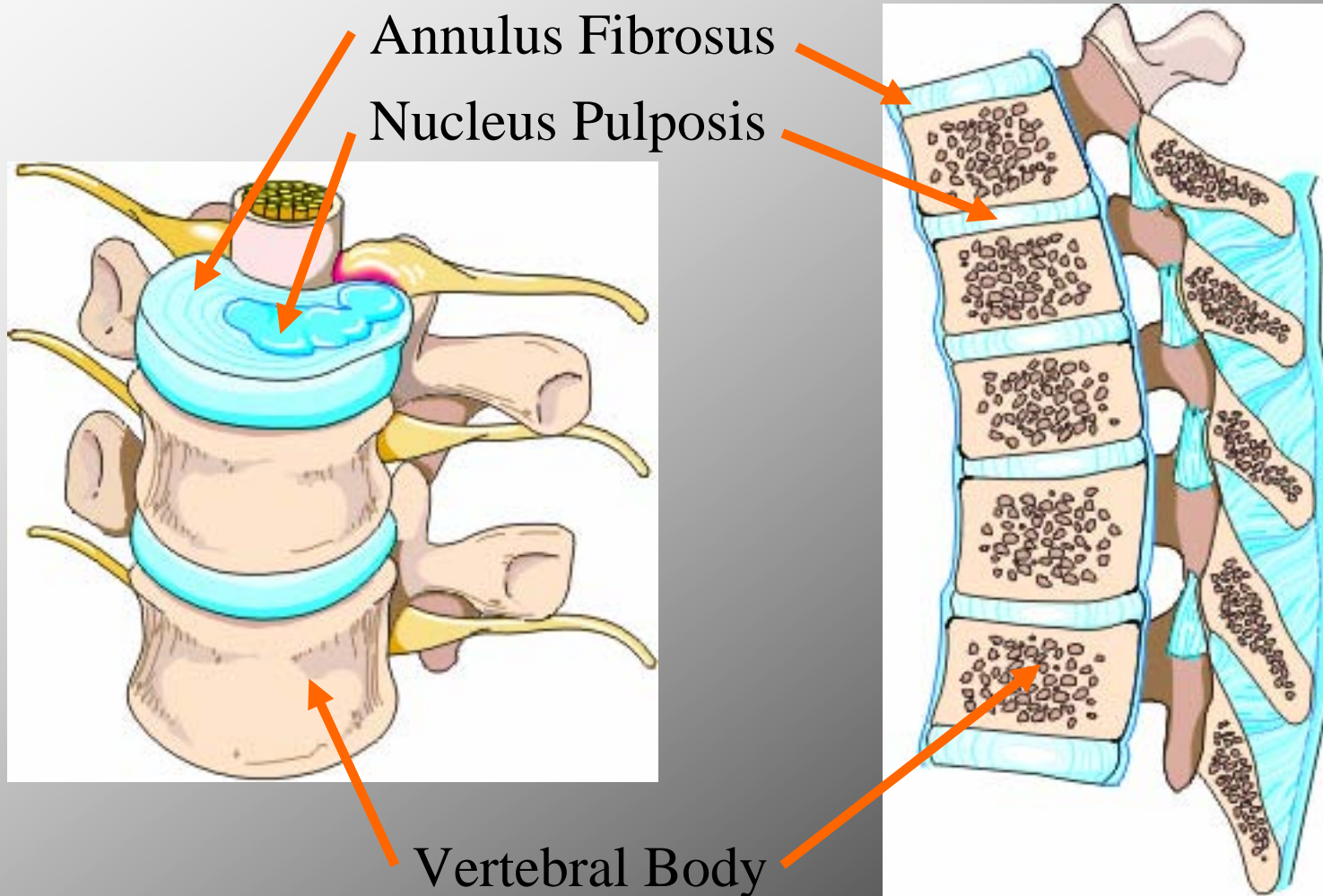
# Army Repeated Jolt Standard

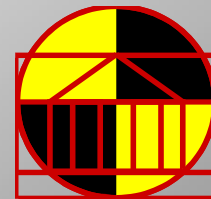
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- Basis of New ISO-2631.5 (Alem-2002)
  - 3D – x, y, z lumbar acceleration
- Predominantly Compressive Loading
  - Limited to +/- 4 g
- Likely the ‘Best’ Option Available
  - Accounts for repetitive loading
  - Columnar spinal loading
  - Does not account for complex postures/complex modes of motion
  - Neural net dynamics model
  - **Based on spinal fracture**



# Lumbar Spine Biomechanics





# Lumbar Spine Biomechanics

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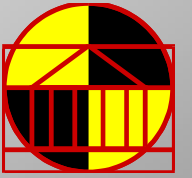
- Experimental Models – Difficult to Fail in Compression
  - Rate Sensitive (Tsai, *et. al.* – 1998)
    - Increased Loading Rate => Increased Injury
  - Minor damage to vertebral body increases loading (Adams *et. al.* – 2000)
  - Lateral motions – higher interdisc stress (Dolan-2001)
  - *Repeated flexion/extension with small compression may cause herniation (Callaghan et. al. – 2001)*



# Summary

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- No Perfectly Suitable ‘Biomechanical’ Model for Repeated Low-Level Impact
  - All based on gross body acceleration or spinal fracture
  
- Need: Material Fatigue Model of Intervertebral Disc Failure
  - Need to Incorporate Flexion/Extension and Lateral Motions into the Model

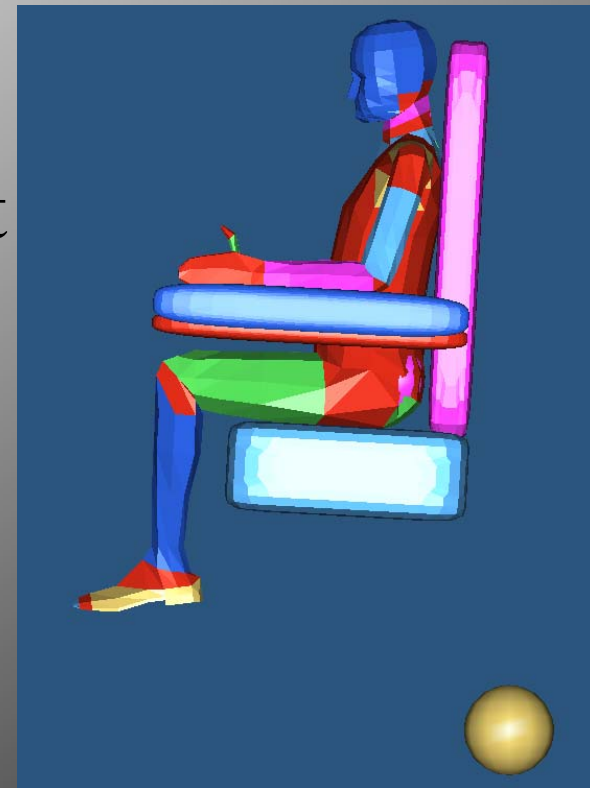


# Madymo Model

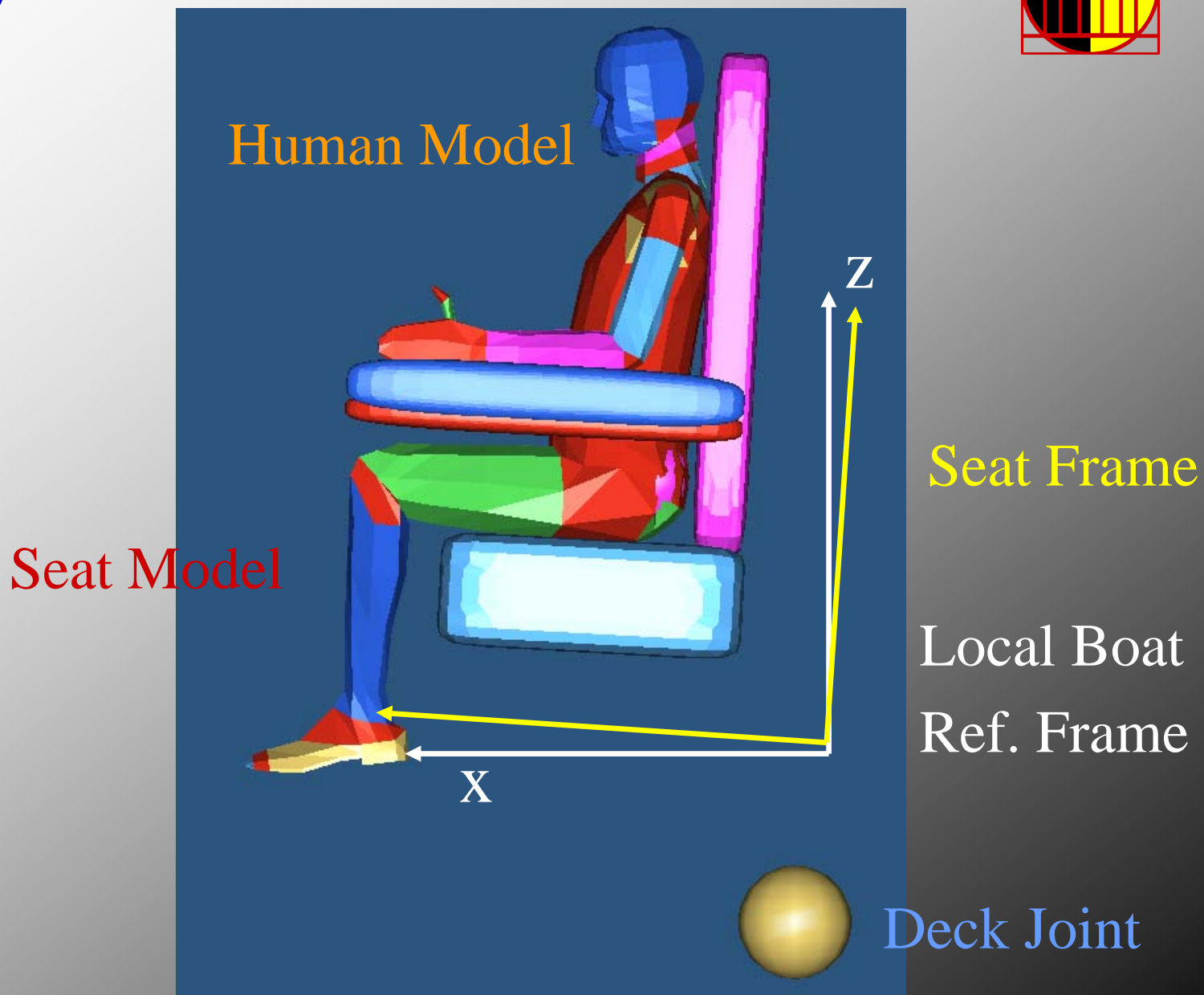
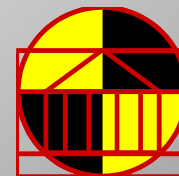
# Overview: Madymo Human Model (MATHematical DYNAMIC MOdel)



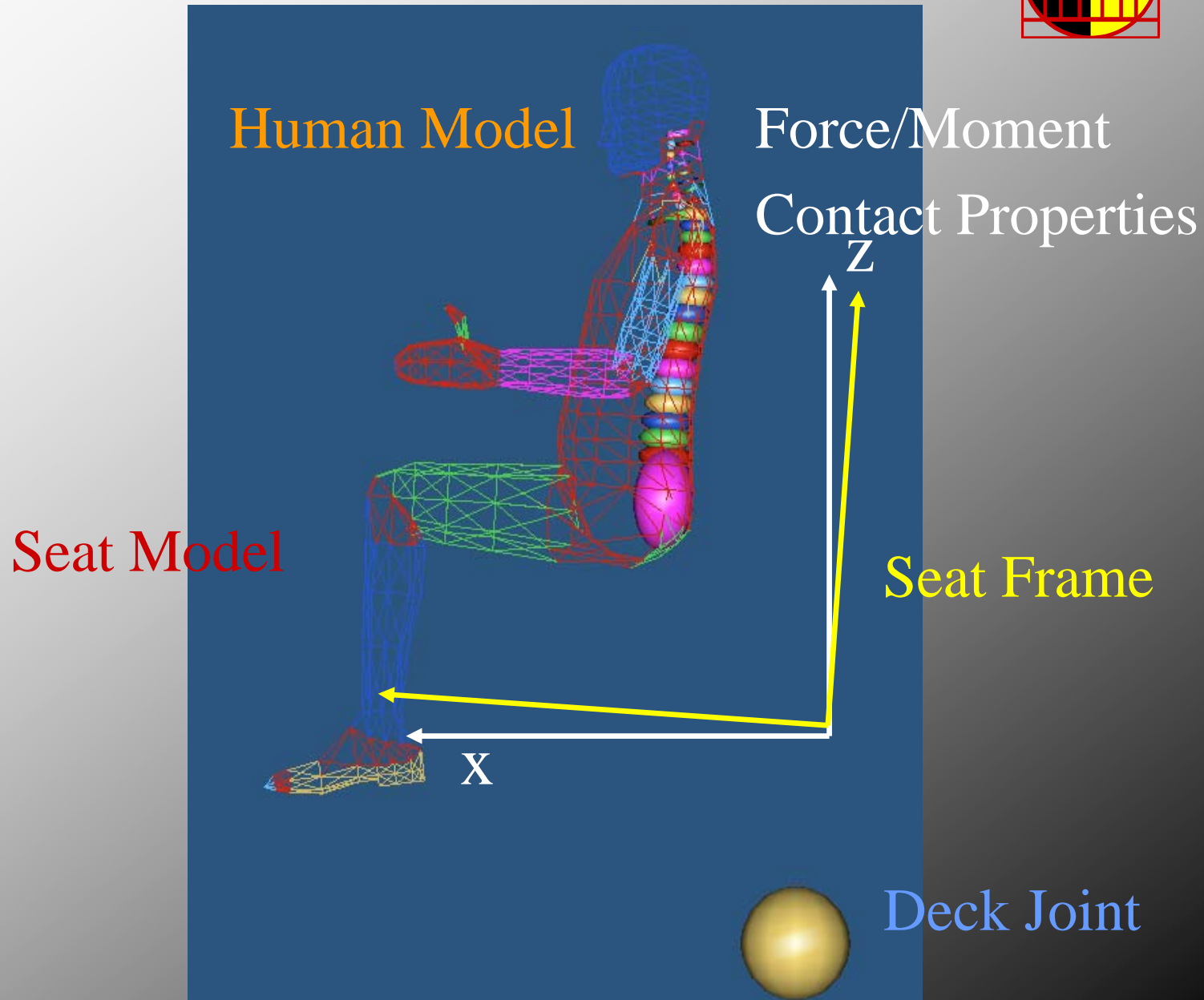
- Simulates dynamic behavior of physical systems
- Validated using vehicle collisions and injury assessment data
- Outputs
  - Force, moment, disp., vel., accel.
  - Injury parameters



# Madymo Human Model



# Madymo Human Model

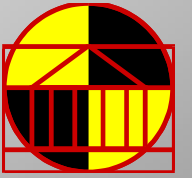




# Validation Dataset – Mk V Data

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- Validation Dataset – 6DOF Data from Sea Trials (January 2002, Peterson, *et al*)
- Four Impacts Chosen – Range of Conditions
  - Intense vertical/horizontal impact loads, lateral, torsion
  - May be repeated over long periods of time
  - Two similar to range of ISO 2631.5 – two outside



# Validation Dataset

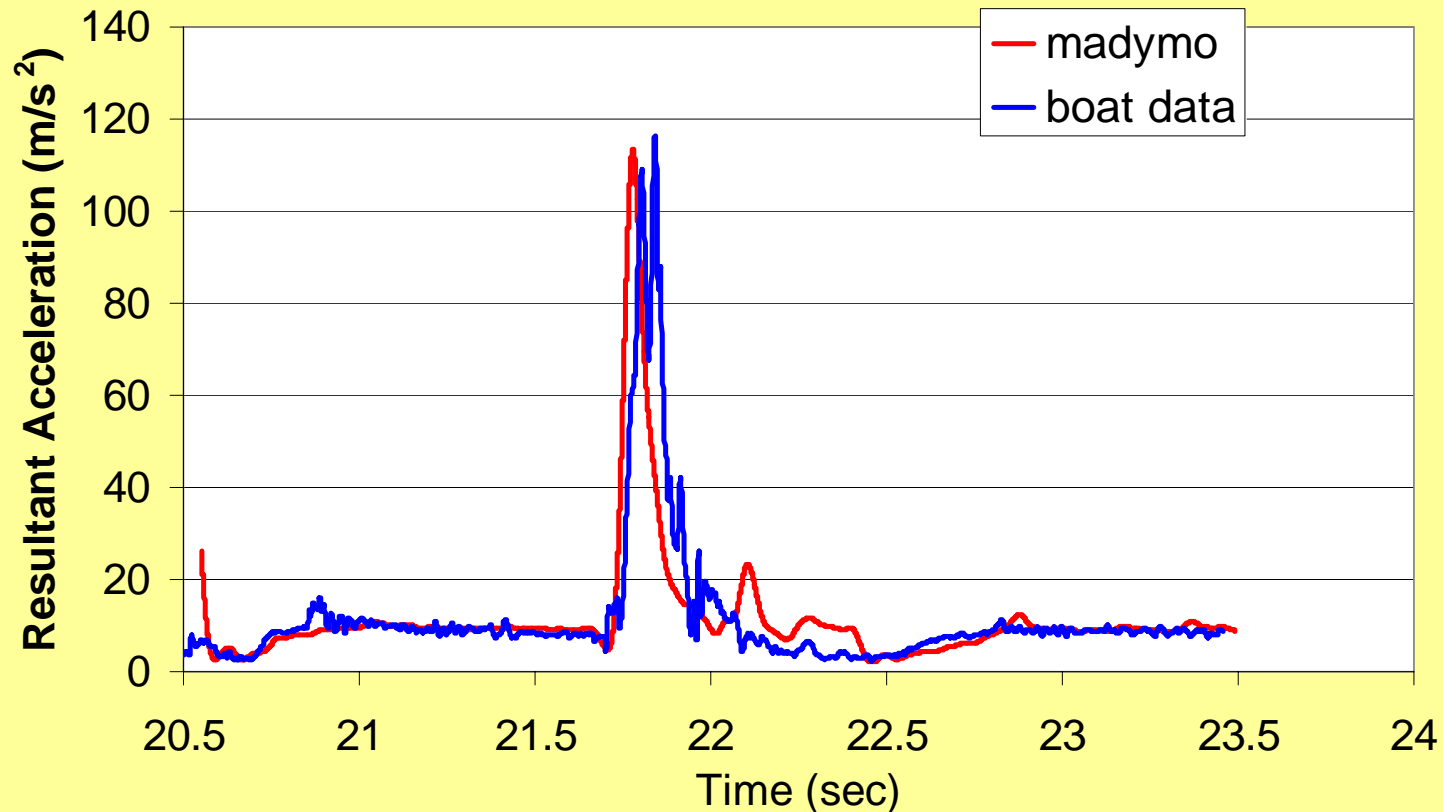




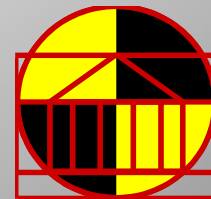
# Madymo Simulation

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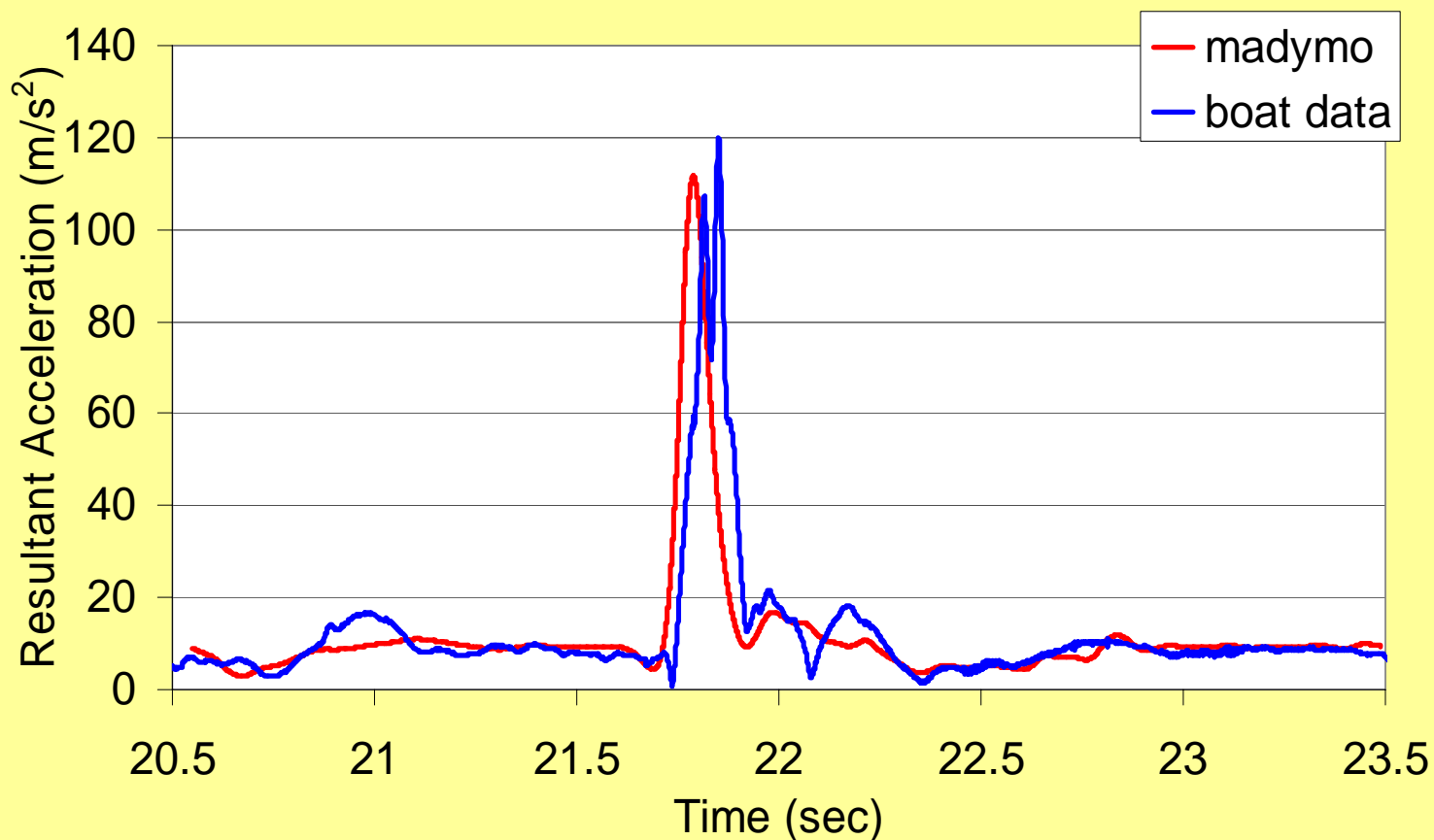
# Compare Experiment with Model Output Dynamics (Lumbar Spine)



'Good' = Peaks within 10%,  
Impulse within 10% of Experimental Values



# Large Pulse - Head CG Accel.

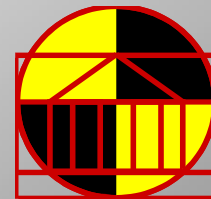




# Madymo 'Metamodel'

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- 'Validated Model'
- Develop 'Metamodel'
  - Run validated Madymo model for range of inputs
  - Deck inputs => Human injury output
  - Rapid calculation
- Metamodel Used to Evaluate Injury In:
  - Computational boat model
  - Tank test boat model
  - Experimental boat



# Validation Dataset Caveat

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- Not Sensitive to Pitch-Related Motions
  - Appear to be relatively small
  - Related to relatively high velocity, relatively low sea state?
- Relative contribution of pitch vs. translational velocity
  - *Repeated flexion/extension with small compression may cause herniation (Callaghan et. al. – 2001)*

# Effect of Pitch

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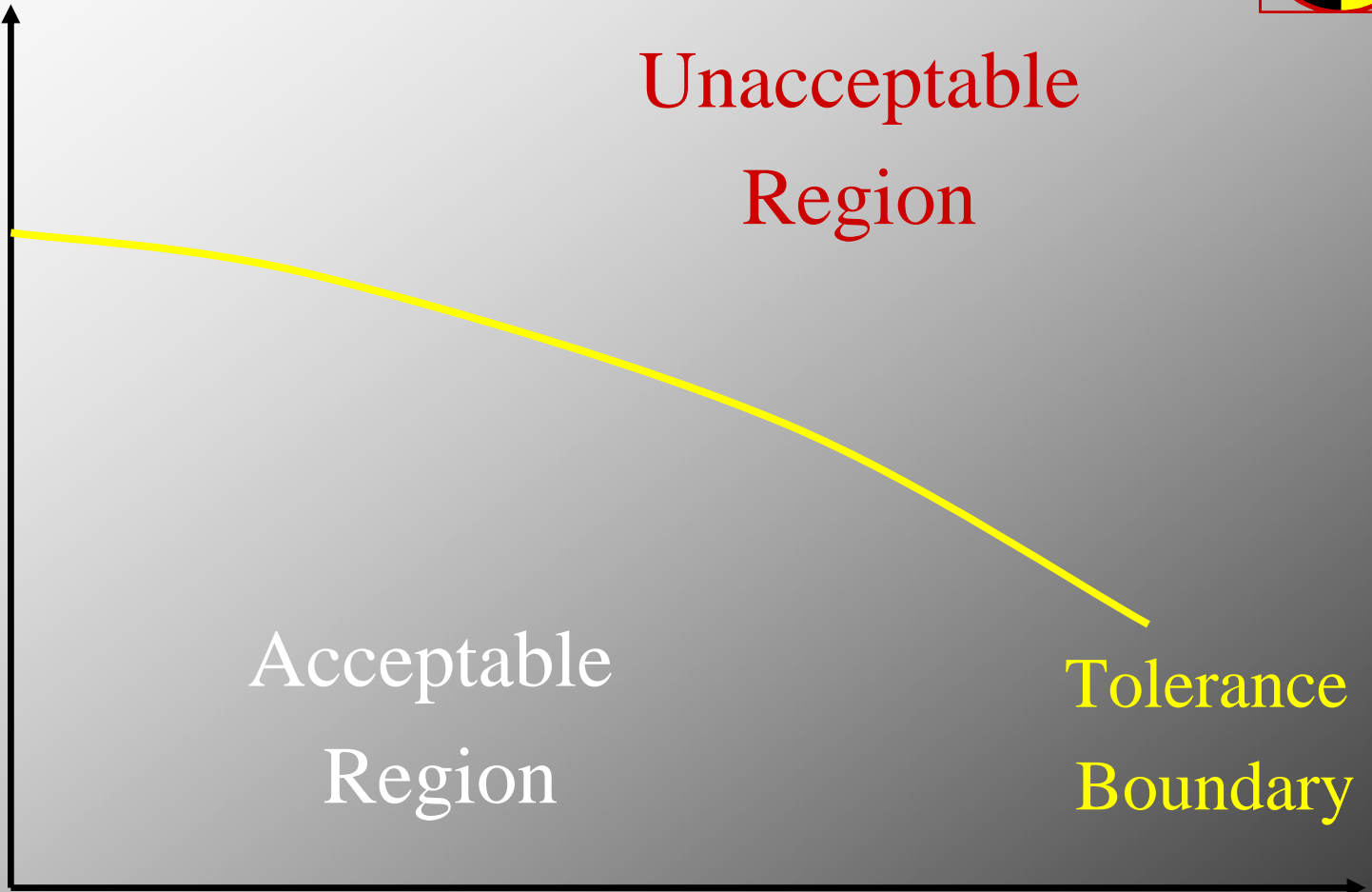
Unacceptable  
Region

Boat  
Speed

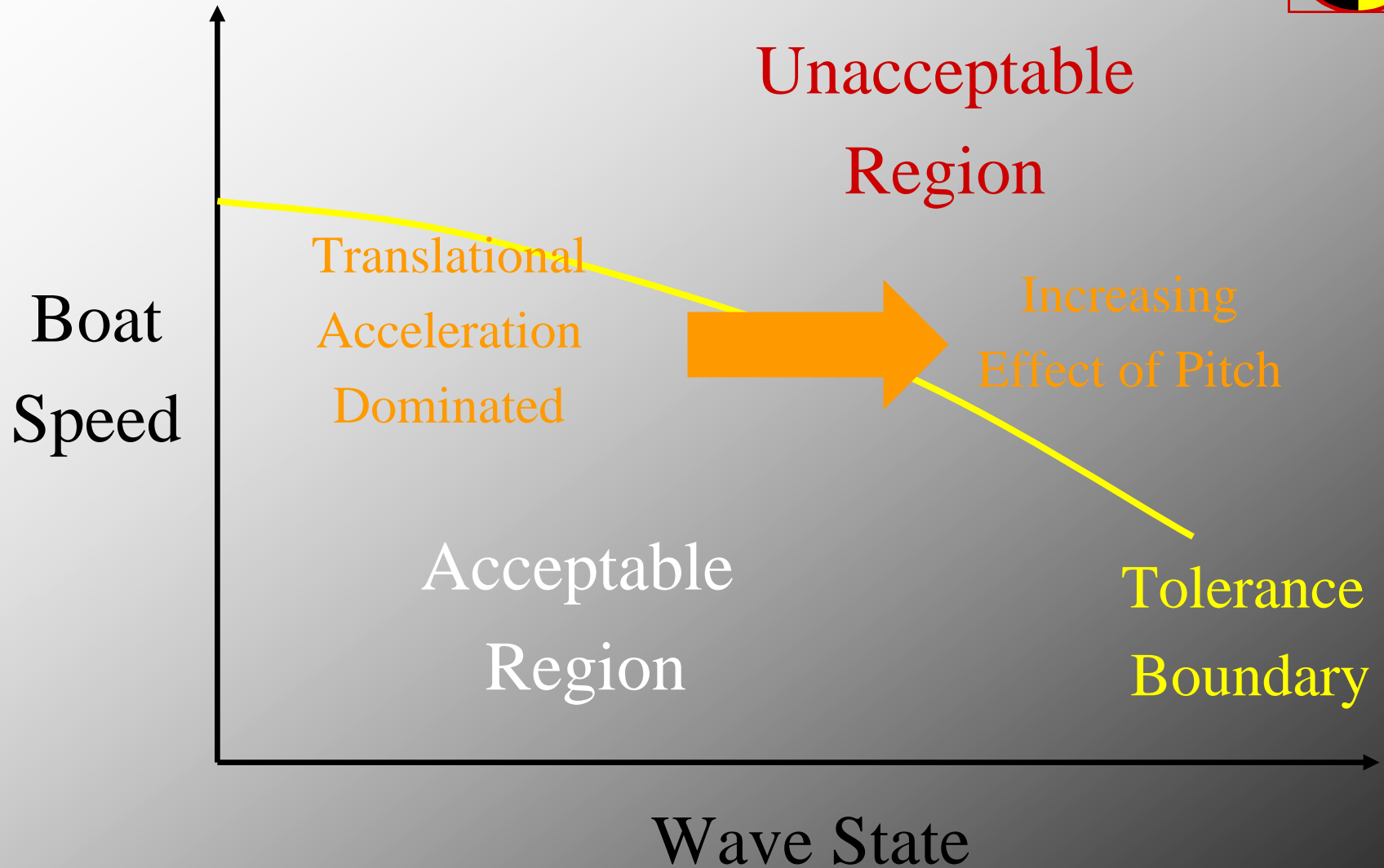
Acceptable  
Region

Tolerance  
Boundary

Wave State



# Effect of Pitch

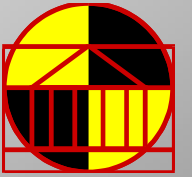




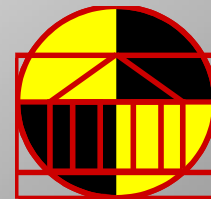
# Uses and Limitations

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- Calculation of injury in design/construction/deployment phases of boat lifetime, e.g.:
  - Explore seats/belts/countermeasures
  - Incorporate into naval architecture codes
  
- Limitations
  - Only as good as validation studies
  - Local moments and forces approximate
  - Significant limitation of the injury model
    - Not based on injuries identified in epidemiological studies

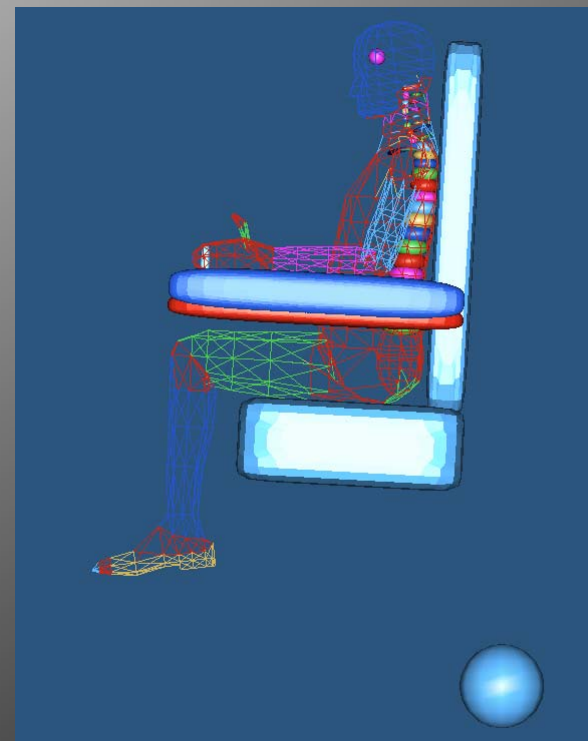
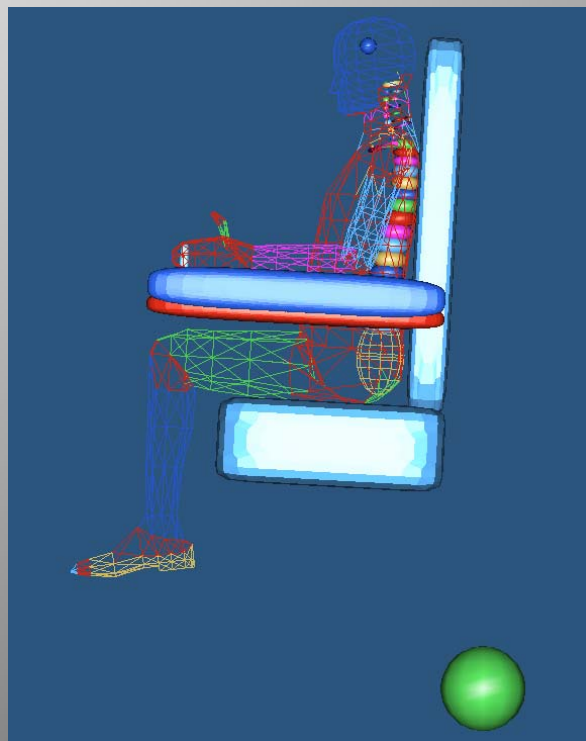
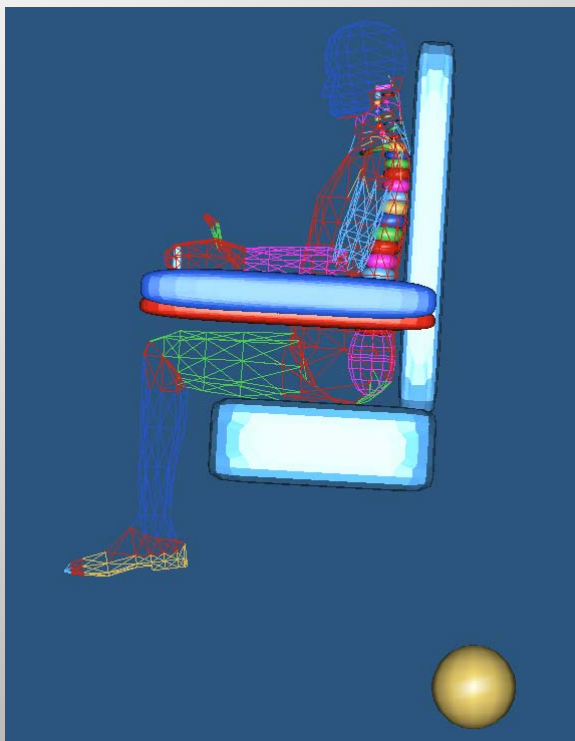


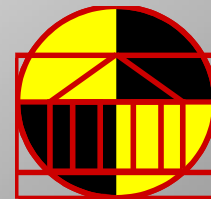
# Example: Exploratory Study



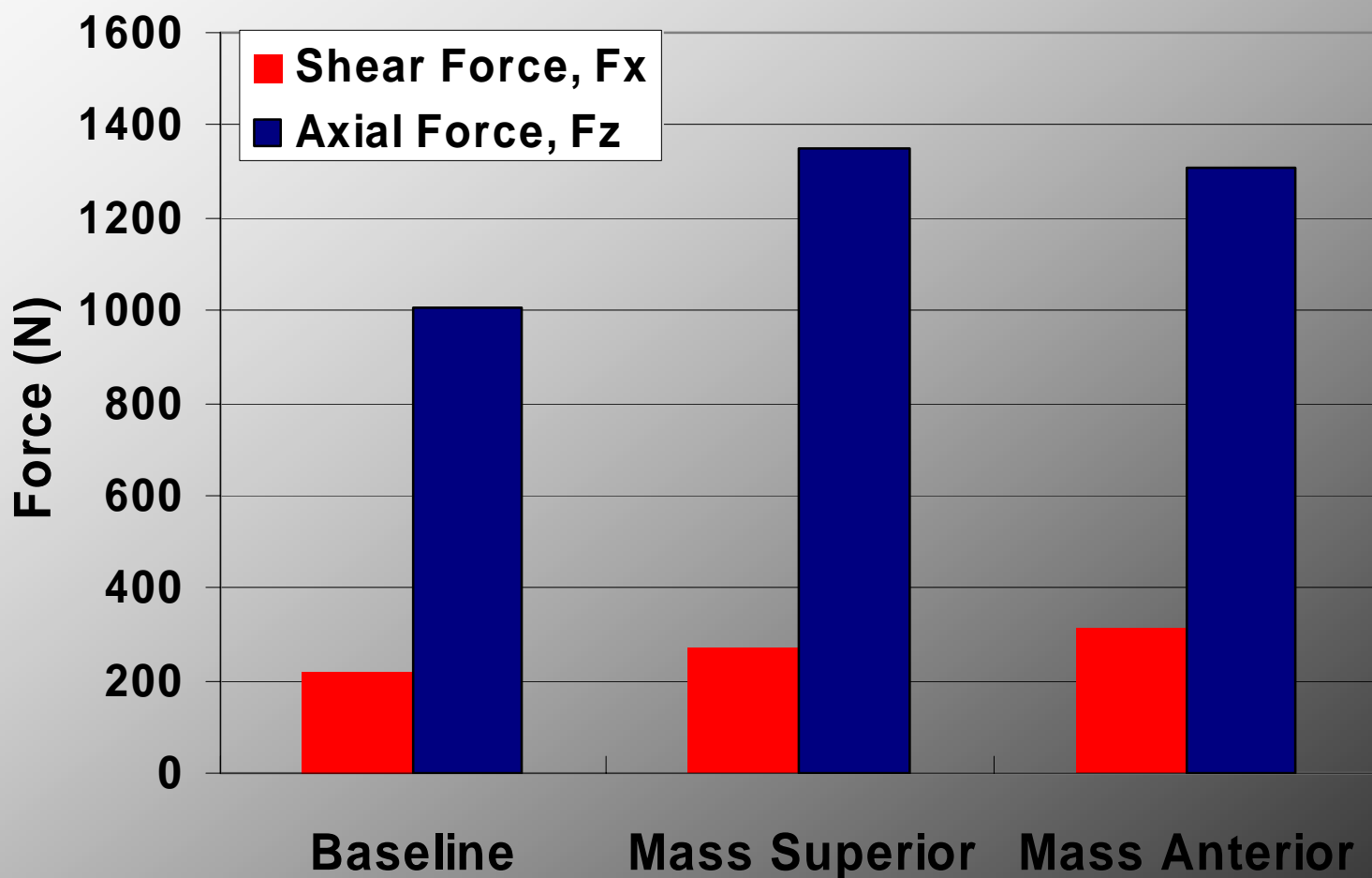
# Head Supported Mass (HSM)

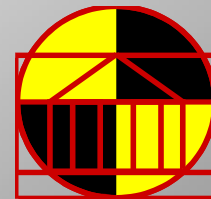
- No Mass
- 1.75 kg at 52 mm Superior to Head CG
- 1.75 kg at 17 mm Anterior, 49 mm Superior



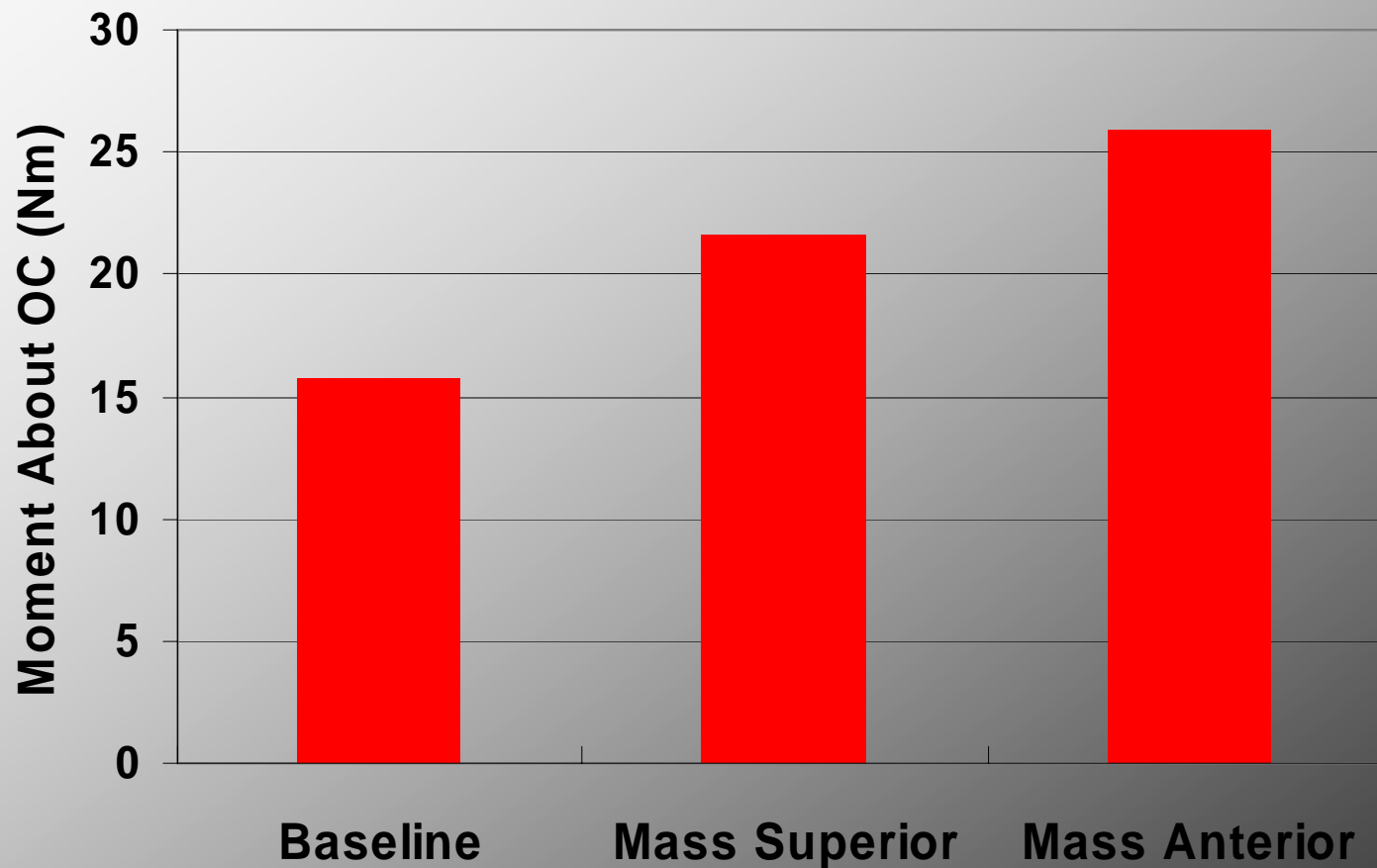


# Effect of HSM on Neck





# Effect of HSM on Neck



Injury Criterion for Flexion: 190 Nm



# Current Work

- Validate Using Current Datasets
  - Higher sea states
  - More rotation
- Validate Against Dummy Data in High Speed Craft
- Develop Madymo ‘Metamodel’
  - Fast calculation code for parameter studies





# Summary

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- No Current Injury Model is Fully Applicable
- Framework
  - Robust injury model needed!
  - Numerical modeling
    - Evaluation of concepts, countermeasures, etc.
    - Development of specifications
  - Experimental verification/validation
    - Volunteer experimental studies
    - Mechanical performance characterization
  - Epidemiological tracking



# Acknowledgements

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- U.S. SOCOM
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- UVa – School of Engineering and Applied Sciences



# Source

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University of Virginia.